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Rapid Communication

In vitro skin penetration of propranolol enantiomers

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Summary

Transfer rates of individual enantiomers of propranolol across human skin were determined in vitro. Percutaneous penetration of propranolol from propylene glycol was negligible at the concentration previously reported to show enantioselective transfer in rat skin. Transfer of (*R*)- and (*S*)-propranolol from aqueous solutions of both the racemate and the pure enantiomers showed no differences in the rates of penetration demonstrating that the rate of transfer of propranolol across human skin from these solutions was independent of the stereochemistry of the drug. In addition there was no evidence for racemisation during the transfer process.

The transdermal delivery of many drugs has received considerable attention in recent years. However, surprisingly little attention has been paid to the transfer characteristics of individual enantiomers of chiral species. This is an important issue in view of the fact that significant differences are frequently found between the activities of drug enantiomers (e.g., Stevenson and Williams, 1988). As a consequence, regulatory authorities are demanding more information concerning all aspects of the administration of chiral drugs (Bridges, 1991), including those delivered transdermally.

Miyazaki et al. (1992) recently reported marked differences in the transfer rates of the enan-

tiomers of the β -blocking drug propranolol (as free base) across rat skin and claimed that the process responsible for enantioselectivity resided within the stratum corneum. This communication describes similar experiments on the individual *R* and *S* enantiomers and the racemate using full-thickness excised human skin.

The (\pm)-propranolol hydrochloride (determined enantiomeric ratio 1.21:1, *R*:*S*) was a gift from ICI Pharmaceuticals plc. Enantiomerically pure (*R*)- and (*S*)-propranolol hydrochlorides were obtained from Cambridge Research Biochemicals Ltd, Northwich, U.K. Free propranolol base was prepared by neutralisation of an aqueous solution of the hydrochloride salt with 2 M sodium hydroxide. Sodium perchlorate was obtained from Aldrich. All other materials were AnalaR grade. Human male abdominal skin was obtained post-mortem.

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After removal of subcutaneous fat by blunt dissection the skin membranes were mounted, stratum corneum uppermost, in all-glass Franz-type calibrated diffusion cells of nominal diffusional area 0.8 cm^2 and receptor volume 2.2 cm^3 . The receptor chambers were filled with pre-thermostatted phosphate-buffered saline (PBS) and the cells immersed in constant temperature water baths at 37°C such that the skin temperature was $32 \pm 1^\circ\text{C}$. The receptor phases were continuously agitated by magnetic followers impelled by submersible multiple stirrer plates. After equilibration for 2 h, 1 ml of the relevant solution was added to the donor compartment which was then capped. At appropriate time points, $200 \mu\text{l}$ was withdrawn from each receptor chamber and retained for analysis. An equal volume of pre-equilibrated PBS was added to maintain the correct volume. A total of five replicates were used for each test.

Initially $100 \mu\text{g ml}^{-1}$ propranolol base in propylene glycol was applied to mimic the conditions employed by Miyazaki et al. (1992) with rat skin. Because the observed transfer rate was very low under these conditions, 0.01 M ($2958 \mu\text{g ml}^{-1}$) solutions in PBS (Green, 1988) of either (*R*)-, (*S*)- or racemic propranolol hydrochloride were also examined.

All samples were analysed by HPLC under the following conditions: LDC analytical constaMetric 3500 pump, LDC analytical membrane degasser, LDC analytical spectroMonitor 5000 detector (289 nm), Promis II autosampler with $100 \mu\text{l}$ loop, Daicel OD-R reversed-phase chiral column (derivatised cellulose/octadecyl), mobile phase 0.5 N sodium perchlorate/acetonitrile (60:40), flow rate 1 ml min^{-1} . Enantiomeric resolution was complete and the *R*(d) form had a shorter retention time than the *S*(l) form. A typical chromatogram is shown in Fig. 1.

When $100 \mu\text{g ml}^{-1}$ propranolol base in propylene glycol was used as donor phase, the quantity of drug found in the receptor chamber at the end of the experiment (72 h) was insignificant, certainly insufficient to determine the enantiomeric ratio. Although this result was contrary to the findings of Miyazaki et al. it is consistent with observations that rat skin is often considerably

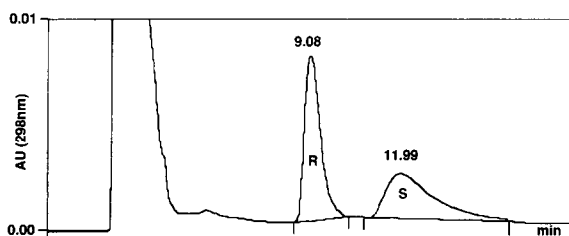
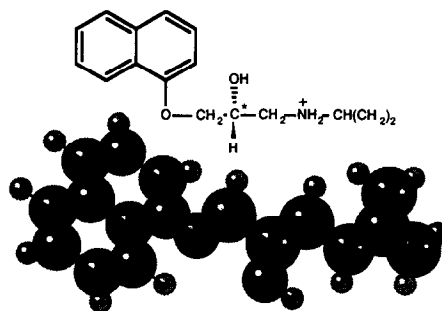


Fig. 1. Chemical structure of propranolol and typical HPLC chromatogram demonstrating complete enantiomeric resolution.

more permeable than human skin (Kao et al., 1985; Scott et al., 1987).

Fig. 2 shows the percentage of the dose of propranolol transferred from PBS solutions of the individual *R* and *S* enantiomers. No difference in transfer rate was apparent and in addition no racemisation was observed. These results were reinforced by the data in Fig. 3 from a PBS

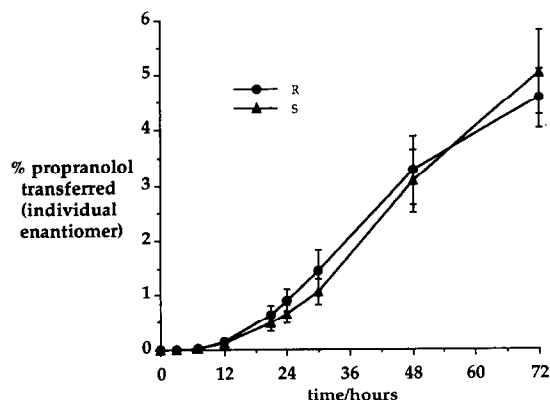


Fig. 2. Percentage propranolol transferred as pure enantiomer.

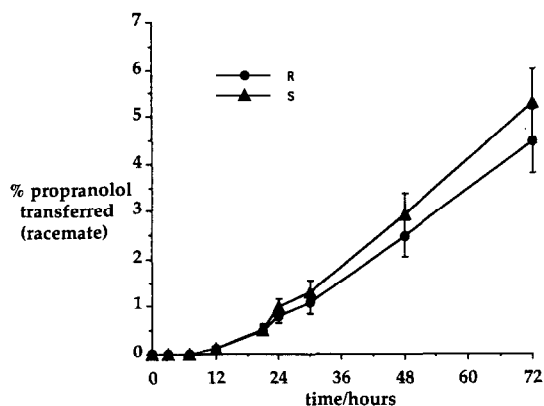


Fig. 3. Percentage propranolol transferred from racemate.

solution of (\pm)-propranolol (correcting for *R* excess). Table 1 gives the steady-state flux and permeability coefficient data. Using analysis of variance no statistically significant differences were found between the transfer characteristics of the enantiomers.

Enantioselectivity might be expected to be particularly sensitive to small changes in molecular environment such as pH and vehicle. The pK_a of propranolol is 9.2. On solution of propranolol free base in propylene glycol the degree of protonation would be minimal, although protonation may occur on contact with the acidic environment (\sim pH 5.5) of the skin surface. On the other hand, propranolol will exist almost entirely in its protonated form (Fig. 1) when in a buffer solution of pH 7.4. The distance between the amine group in propranolol and the chiral centre is quite small and protonation of this group may

interfere with a stereospecific interaction involved in percutaneous transport. However, it has been observed previously (Heard et al., 1992) that enantioselective ion-pair transfer of propranolol is possible using an artificial solid-supported liquid membrane containing a stereospecific carrier molecule.

Alternatively, human stratum corneum may not contain an enantioselective feature which is present in rat skin. This has significant implications where animal skin is used as a predictive model for human skin and the possibility of species differences in transdermal enantioselectivity requires further investigation.

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TABLE 1

Steady-state flux and permeability coefficient values for transfer of propranolol enantiomers across human skin

Enantiomer type		Flux ($\mu\text{g cm}^{-2} \text{ h}^{-1}$)	<i>p</i>	Permeability coefficient ($\times 10^{-3} \text{ cm h}^{-1}$)	<i>p</i>
Racemate	<i>R</i>	1.81 ± 0.27	0.82	1.12 ± 0.17	0.51
	<i>S</i>	1.73 ± 0.25		1.30 ± 0.19	
Individual	<i>R</i>	4.49 ± 0.67	0.21	1.14 ± 0.14	0.20
	<i>S</i>	3.37 ± 0.43		1.52 ± 0.23	

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